

Measuring the Oxygen Volumetric Mass Transfer Coefficient ($k_L a$) of the BioBLU® 1c Single-Use Bioreactor

Igor Vassilev¹ and Ma Sha²

¹Eppendorf Bioprocess Center, Juelich, Germany

²Eppendorf, Inc., Enfield, CT, USA

Contact: bioprocess-experts@eppendorf.com

Abstract

The volumetric mass transfer coefficient ($k_L a$) describes the transfer rate of a gas from the gas phase into the bioreactor medium. In aerobic bioprocess applications, $k_L a$ is a critical parameter for the evaluation of the efficiency of a bioreactor in terms of how effectively oxygen is supplied to the cultured organism. This short protocol describes the detailed procedure of how to measure $k_L a$ of the Eppendorf cell culture bioreactors via the gassing-out method. The $k_L a$ values are influenced by many factors such as the reactor and impeller geometry, medium characteristics, and reactor operation (especially agitation and gassing).

The change of a single factor will result in a change of the $k_L a$ value. As an example, this protocol describes the oxygen $k_L a$ measurement of BioBLU® 1c Single-Use Bioreactors at an impeller tip speed range between 0.1 and 1 meter per second (m/s) and a gassing rate between 5 and 60 standard liters per hour (sL/h). For instance, at 0.5 m/s and 25 sL/h the BioBLU 1c with one impeller shows a $k_L a$ value of $5.39 \pm 0.38 \text{ h}^{-1}$. This short protocol can serve as a reference for the bioprocess professionals who are interested in $k_L a$ measurement of the large collection of Eppendorf cell culture bioreactors.

Introduction

The volumetric mass transfer coefficient ($k_L a$) is a parameter that describes the efficiency of the gas-liquid mass transfer in a bioreactor. The ' $k_L a$ ' is expressed as the rate of molecular diffusion through the gas-liquid interface area ' a ' per liquid volume. The $k_L a$ is defined by the geometrical properties of the reactor and the operational process aspects. It is a powerful parameter to provide information about gas supply limitations in a bioreactor, in particular for oxygen in aerobic processes. The $k_L a$ values can be used for comparison of the performance of bioreactors with similar designs or scale-up strategies [1].

Several methods using reagents or organisms were developed to measure $k_L a$ values [2]. This protocol describes the gassing-out method recommended by the German Society for Chemical Engineering and Biotechnology (DECHEMA) which is an easy and relatively quick method without the need for hazardous chemicals or organisms [3].

As organisms are not needed in this cost-effective method, the experiments can be carried out under non-sterile conditions and without medium exchange for several experiments. It is suggested to use $1 \times$ phosphate-buffered saline (PBS) buffer at 37 °C as a closer representation of

cell culture medium than water. The method is based on dynamic measurements of oxygen concentration. The first step includes the establishment of anaerobic conditions by gassing the PBS buffer with nitrogen. Next, nitrogen gassing is stopped, the reactor headspace is replaced with air (21% oxygen), and the PBS buffer is sparged with air at certain flow rates of interest. By monitoring the dissolved oxygen concentration in the PBS buffer as it rises from the minimum to its equilibrium value, the k_La value can be calculated. Removing excess nitrogen from the headspace before the actual k_La measurement ensures defined

atmospheric conditions in the headspace and reliable preconditions for k_La measurements [3].

This short protocol is designed mainly to measure k_La values of cell culture bioreactors with typical small k_La values as the measurement is done under slow agitation and low gassing rates to mimic real cell culture conditions with minimized shear stress. To provide readers with realistic examples, the short protocol also includes the determination and comparison of k_La values of BioBLU® 1c Single-Use Bioreactors with one impeller (Figure 1).



Figure 1: (A) BioBLU 1c Single-Use Bioreactors were used for k_La measurement in combination with the (B) DASGIP® Parallel Bioreactor System to control the relevant bioprocess parameters.

Learn more about of the BioBLU Single-Use Bioreactors at: <http://www.eppendorf.link/single-use-bioreactors>

Material and Methods

1. Materials

1.1. Assembly Equipment

The protocol can be used for either an Eppendorf autoclavable glass bioreactor or a BioBLU Single-Use Bioreactor. In this example, we used a BioBLU 1c Single-Use Bioreactor with one impeller (Eppendorf Catalog No. 1386111000) with a DASGIP Bioblock (Eppendorf Catalog No. 76DGTBLOCK) including a DASGIP TC4SC4-B module for cell culture with a agitation speed range of

30 – 1,250 rpm (Eppendorf Catalog No. 76DGTC4SC4B), DASGIP PH4PO4RD4L sensor module (Eppendorf Catalog No. 76DGPH4PO4RDL) and a DASGIP MX4/4 module with an air gassing range of 0.5 – 250 sL/h (Eppendorf Catalog No. 76DGMX44H).

Alternatively to the modular system, a BioFlo® 320 (Eppendorf Catalog No. 1379963011) can also serve as a controller for k_La measurements. For high gassing accuracy, a thermal mass flow controller for cell culture applications with a gassing range of 0.12 – 60 sL/h (0.002-1.0 SLPM) is

recommended to be used with the BioFlo 320 bioprocess controller. In this example, we used Hamilton® OxyFerm FDA 225 Analog polarographic DO sensors (12mm diameter with 225 mm insertion depth, Eppendorf Catalog No. 78108039). Furthermore, the SciVario® twin (Eppendorf Catalog No. 7600100001) equipped with the DASware® control software can serve as an additional alternative bioprocess controller.

1.2. Chemicals

Phosphate Buffered Saline tablets were used for 1 × PBS medium preparation (Gibco PBS-Tablets, Thermo Fisher Scientific).

2. Experimental procedures

2.1. Bioreactor assembly

Assemble the glass bioreactor according to the user manual or take a ready-to-use BioBLU Single-Use Bioreactor. Fill the bioreactor with 1 × PBS to its maximum working volume.

2.2. DO sensor calibration

Install the appropriate polarized analog DO sensor onto the bioreactor head plate and calibrate the sensor. Set the temperature at 37 °C and agitation at the maximum agitation rate of the bioreactor recommended by the user manual. Sparge gas composed of 100% nitrogen into the bioreactor at the maximum gassing rate of the bioreactor control system. When DO reading stabilizes, set zero (0%). Then change the gas composition to sparge 100% air into the bioreactor at 1 vessel volume per minute (vvm) or at the maximum gassing rate of the bioreactor control system, and wait for the DO reading to stabilize to set the span (100%).

2.3. $k_L a$ measurement for oxygen of Eppendorf cell culture bioreactors

Keep the temperature at 37 °C and agitation of the bioreactor at the maximum agitation rate recommended by the user manual. Sparge gas composed of 100% nitrogen into the bioreactor at the maximum gassing rate of the bioreactor control system until the DO values drop below 10%.

Thereafter, stop agitating or set agitation to the minimum setpoint of the used controller, and flush the head space with 100% air at 0.05 vvm via overlay gassing until the gas in the headspace has been exchanged at least three times.

Continue headspace gassing and start data acquisition with a control software. Immediately start agitation and submerged gassing with 100% air at impeller tip speeds and gassing rates of interest depending on needs, controller selection and

bioreactor choice. For example, when using a BioBLU 1c Single-Use Bioreactor with a DASGIP Bioblock, the impeller tip speed and gassing rate can range from 0.1 to 1 m/s, and from 1 to 60 sL/h, respectively. The measurement can be stopped when the DO measuring reaches values over 90%. Carry out the experiment at least three times to provide a mean $k_L a$ of the bioreactor ideally with a standard deviation below 10%. Repeat the $k_L a$ measurements under a broad range of process operation conditions varying gassing rates and agitation to evaluate the behavior of $k_L a$ at different cell culturing conditions. The experimental conditions of selected examples are summarized in Table 1.

Table 1: Process parameters applied for $k_L a$ measurement

Parameters	Configuration
Bioreactor	Autoclavable cell culture glass bioreactor or a BioBLU 1c Single-Use Bioreactor
Drive	Direct drive or magnetic drive
Working volume	Maximum working volume of the bioreactor
Impeller tip speeds	0.1 - 1 m/s
Agitation direction	Clockwise or counterclockwise
Overlay gassing	100 % air at 0.05 vvm
Submerged gassing	100 % air at 1 - 60 sL/h
Temperature	37 °C
Impeller type	Pitched-blade impeller
Sparger	Open pipe or macrosparger

3. Calculations

The $k_L a$ of oxygen in a bioreactor is calculated as follows [3]

$$\text{Equation 1: } \frac{dDO}{dt} = k_L a \times (DO^* - DO)$$

$$\text{Equation 2: } \int_{DO(t=0)}^{DO(t)} \frac{dDO}{(DO^* - DO)} = \int_{t=0}^t k_L a \times dt$$

$$\text{Equation 3: } -\ln\left(\frac{DO^* - DO(t)}{DO^* - DO(t_0)}\right) = k_L a \times (t - t_0)$$

where $DO(t_0)$ is equal to the minimum dissolved oxygen content in the medium (i.e., 0%) and DO^* represents DO at saturation (i.e., 100%). $DO(t)$ is the measured DO content (%) in the liquid at each time point t (h). The $k_L a$ value is determined by plotting a linear graph using the left side of Eq. 3 as y-axis values as a function of time with a minimum of seven values between 10 and 90% DO. The $k_L a$ value equals the absolute value of the slope of the graph.

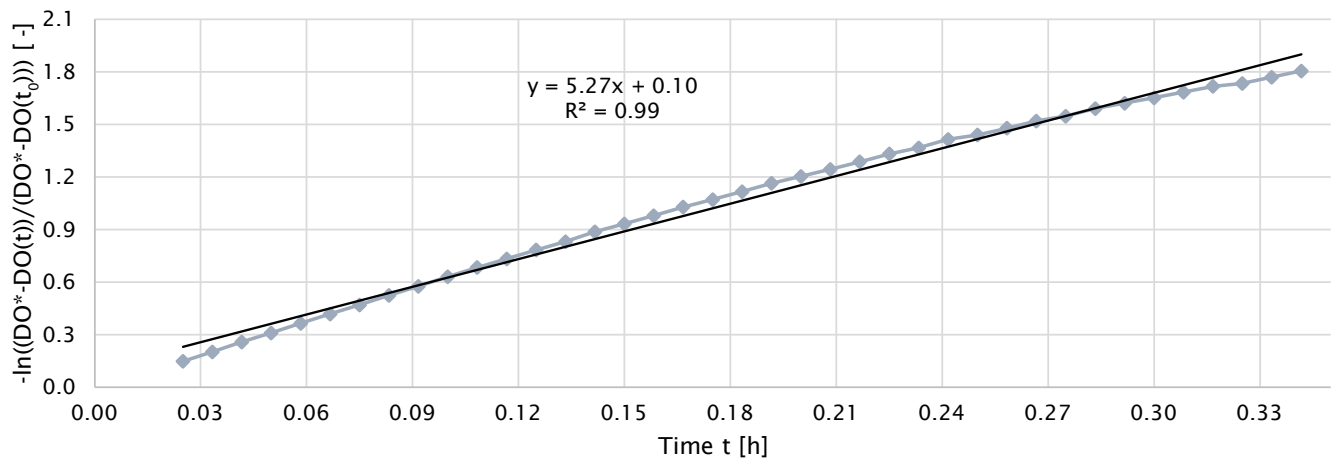


Figure 2: An example (BioBLU 1c with one impeller, 0.5 m/s, 25 sL/h) of plotting the left side of Equation 3 $-\ln\left(\frac{DO^* - DO(t)}{DO^* - DO(t_0)}\right)$ as a function of time to determine the $k_L a$ value. The absolute slope of the graph (5.27) represents the $k_L a$ value with h^{-1} as its unit.

Example of $k_L a$ measurement using BioBLU 1c Single-Use Bioreactors with one impeller

The ready-to-use BioBLU 1c Single-Use Bioreactor was set up as described in the user manual and filled to its maximum working volume with 1 × PBS (i.e. 1250 mL). A polarized Hamilton OxyFerm FDA 225 analog polarographic DO sensor with a diameter of 12 mm and a 225 mm insertion depth was installed in the bioreactor and calibrated via a two-point calibration as follows: the temperature was set to 37 °C, impeller tip speed was set to 600 rpm (1.57 m/s) in clockwise agitation direction, and 100% nitrogen submerged gassing was set to 75 sL/h. After reaching a stabilized DO, the zero point (0%) was set. Then the gassing was changed to 60 sL/h and gas content to 100% air. The DO calibration was finalized by setting the span when the DO reading stabilized (100%).

The oxygen $k_L a$ of the bioreactors was determined at gassing rates of 5, 10, 25 and 60 sL/h, and impeller tip speeds of 0.1, 0.2, 0.5 and 1 m/s. The process of the $k_L a$ determination method can be divided into three phases (Table 2). At the beginning of each $k_L a$ measurement (phase I), the DO was first brought close to 0% by gassing the medium with 100% nitrogen at 75 sL/h (the DASware

control time profile of nitrogen gassing can be seen in Figure 3A) and 600 rpm (1.57 m/s) impeller tip speed (the DASware control time profile of agitation can be seen in Figure 3B). In phase II, the nitrogen gassing was stopped and agitation was set to the minimum of the controller (i.e., to 0.08 m/s tip speed using the DASGIP Bioblock with the DASGIP TC4SC4-B module). The headspace gas of the reactor was replaced with 100% air by overlay gassing with air at 0.05 vvm for 10 min (the DASware control time profile of overlay gassing can be seen in Figure 3C). Afterward (phase III), submerged gassing (100% air at 5 sL/h) was initiated (the DASware control time profile of submerged gassing can be seen in Figure 3D) and overlay gassing was continued at 0.05 vvm. The agitation was immediately started at 0.1 m/s tip speed. The DO changes were recorded every 30 seconds via DASware control, and data acquisition was completed when DO readings reached values over 90%. The measured DO values during DO raise between 10 and 90% were used to determine $k_L a$ by plotting the left side of equation 3 as a function of time. Depending on the linear regression, the chosen spectrum of measured DO values can be adjusted to

a range between 10 and 75% to ensure linear slopes with high R-squared ($R^2 > 0.99$) (Figure 2). However, ensure to use a statistically significant number of DO values ($n > 7$). All three phases need to be repeated in the order listed in Table 2 at least three times (Figure 3) to provide a mean $k_L a$ of the bioreactor at the set impeller tip speed and gassing rate (i.e., 0.1 m/s and 5 sL/h). In this example, a DASGIP Bioblock with DASware control was applied to regulate

the process and record DO data (Figure 3). Alternatively, a BioFlo 320 bioprocess controller could directly be used for process control, data recording and data reading. Figure 4 demonstrates an example of time profiles for submerged nitrogen gassing, agitation, overlay air gassing, and submerged air gassing using the BioFlo 320 controller interface.

Table 2: Time profile of the different phases to measure $k_L a$ at 0.1 m/s tip speed and 5 sL/h air gassing

Phase	Time stamp [h:min:s]	Impeller tip speed/Agitation [m/s]/[rpm]	Submerged 100% nitrogen gassing [sL/h]/[vvm]	Submerged 100% air gassing [sL/h]/[vvm]	Overlay 100% air gassing [sL/h]/[vvm]
I Medium is gased with nitrogen to bring DO close to 0%.	0:01:00	1.57/600	75/1	0	0
	1:01:00	1.57/600	75/1	0	0
II Nitrogen gassing is stopped and agitation is set to the minimum. Headspace gas is replaced with 100% air via overlay gassing.	1:01:01	0.08/30	0	0	3.8/0.05
	1:11:01	0.08/30	0	0	3.8/0.05
III DO is increased via submerged gassing with air and agitation at settings of interest to measure the oxygen transfer rate from the gas phase into the medium.	1:11:02	0.1/38	0	5/0.07	3.8/0.05
	3:11:02	0.1/38	0	5/0.07	3.8/0.05

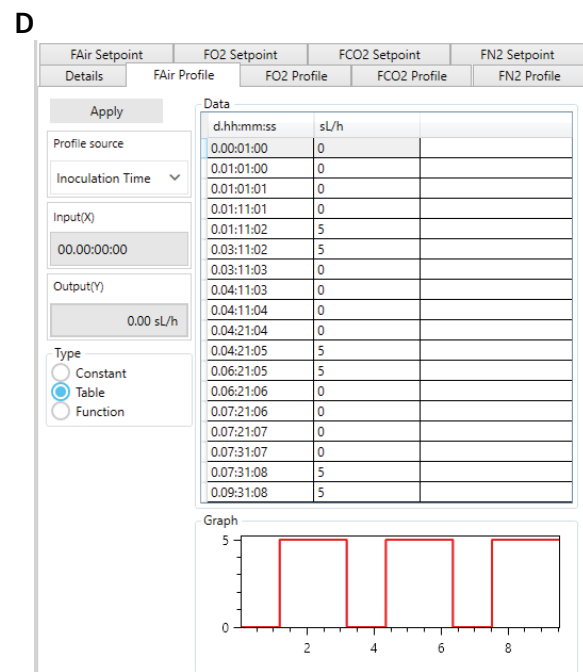
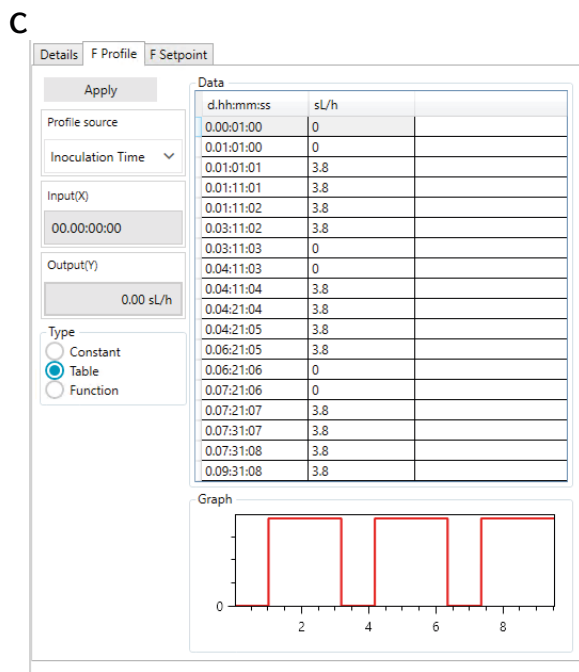
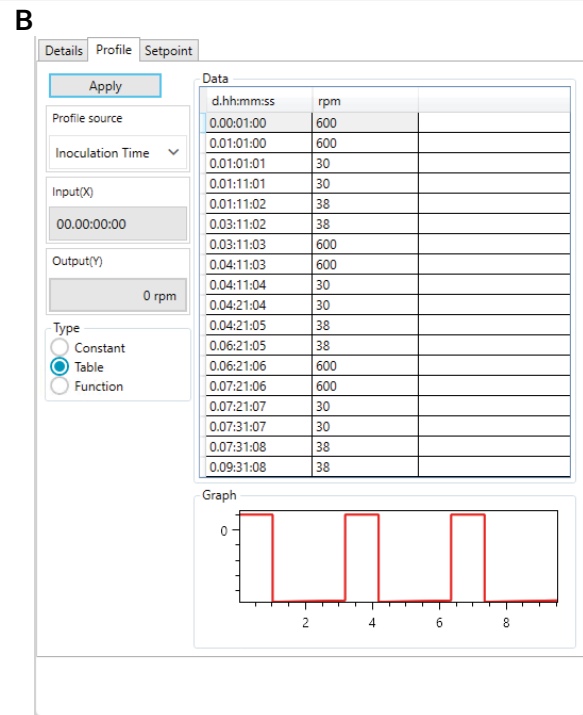
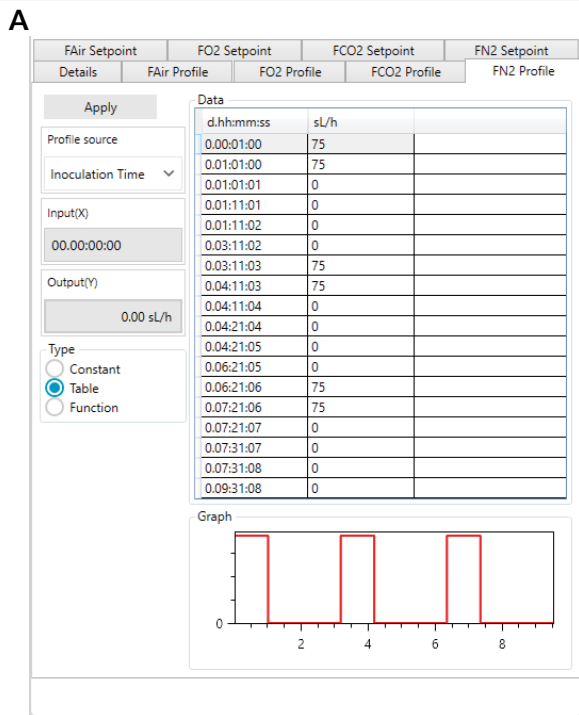


Figure 3: DASware control time profile to measure $k_L a$ in triplicates at 0.1 m/s tip speed and 5 sL/h air gassing: **(A)** Submerged nitrogen gassing, **(B)** agitation, **(C)** overlay air gassing, **(D)** and submerged air gassing.

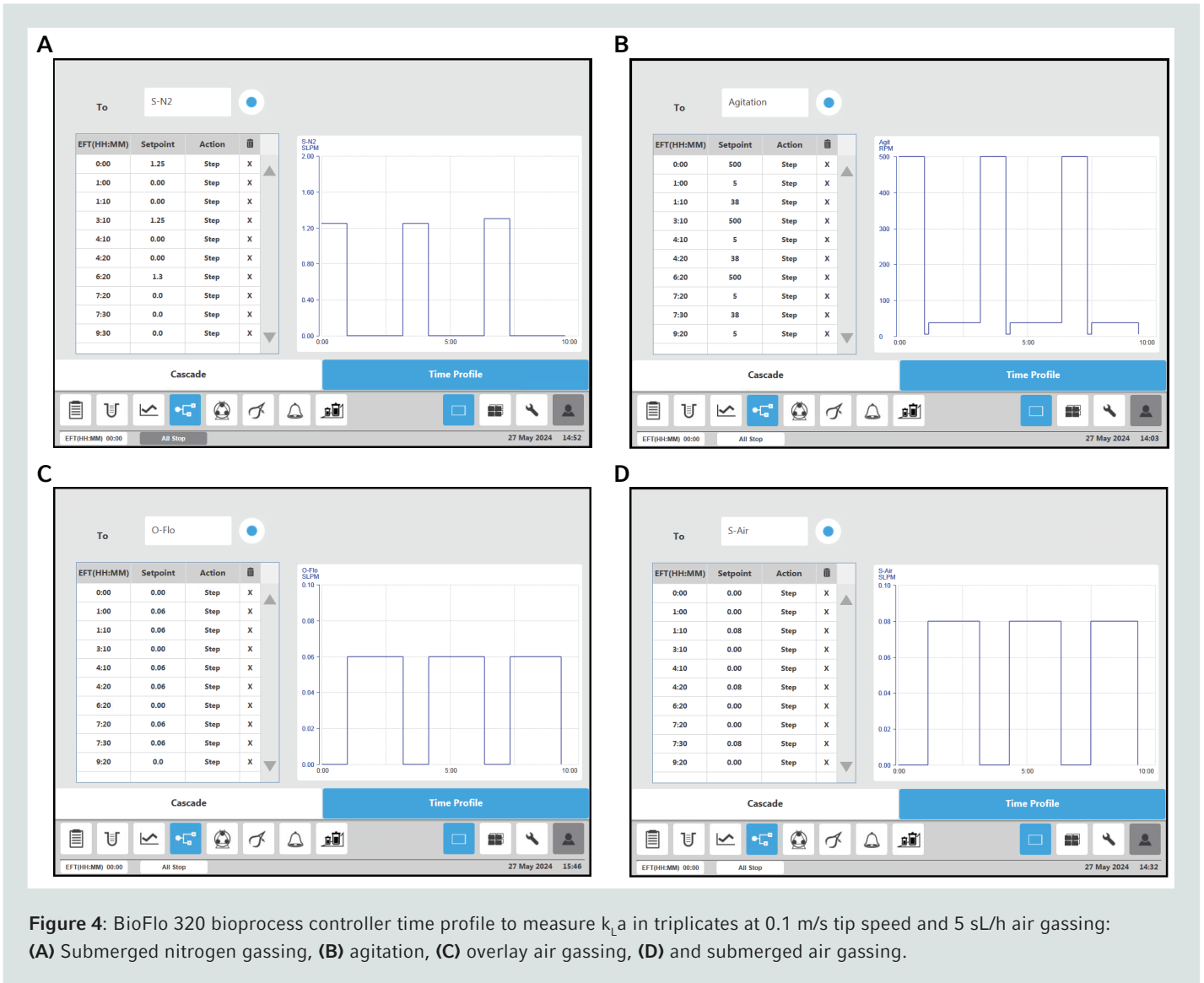


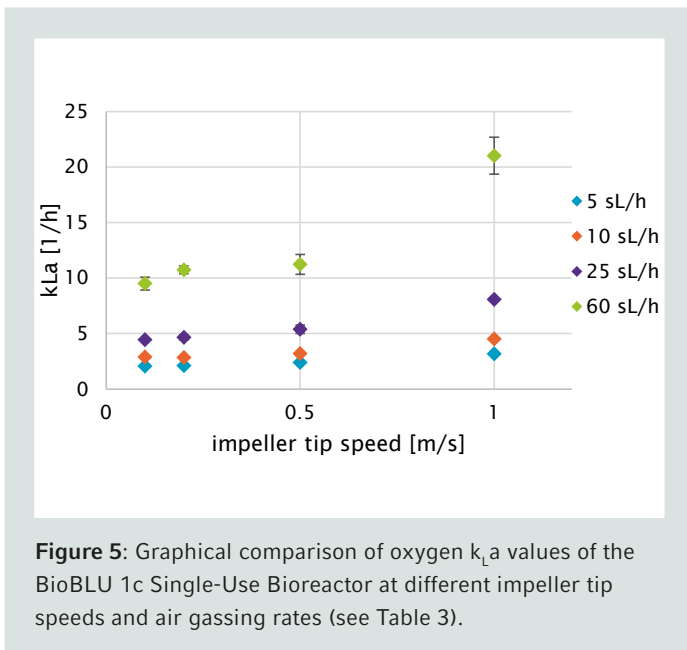
Figure 4: BioFlo 320 bioprocess controller time profile to measure $k_L a$ in triplicates at 0.1 m/s tip speed and 5 sL/h air gassing: (A) Submerged nitrogen gassing, (B) agitation, (C) overlay air gassing, (D) and submerged air gassing.

All procedure steps were repeated for each impeller tip speed (i.e., 0.1, 0.2, 0.5 and 1 m/s) and each gassing rate (5, 10, 25 and 60 sL/h). Table 3 and Figure 5 summarize the

$k_L a$ values measured in triplicates at the different operation conditions.

Table 3: Measured $k_L a$ values of oxygen of the BioBLU 1c Single-Use Bioreactor at impeller tip speeds of 0.1 – 1 m/s and gassing rates of 5-60 sL/h.

Impeller tip speed [m/s]	$k_L a$ [h ⁻¹] at 5 sL/h	$k_L a$ [h ⁻¹] at 10 sL/h	$k_L a$ [h ⁻¹] at 25 sL/h	$k_L a$ [h ⁻¹] at 60 sL/h
0.1	2.06 ± 0.02	2.89 ± 0.03	4.44 ± 0.06	9.51 ± 0.58
0.2	2.11 ± 0.02	2.84 ± 0.02	4.65 ± 0.22	10.74 ± 0.36
0.5	2.40 ± 0.07	3.21 ± 0.01	5.39 ± 0.38	11.24 ± 0.9
1.0	3.18 ± 0.08	4.52 ± 0.09	8.09 ± 0.07	21.02 ± 1.66



The determined oxygen k_La values of the BioBLU 1c Single-Use Bioreactors grew with increasing gassing flow rates and agitation. The k_La values ranged from 2.06 ± 0.02 to $5.39 \pm 0.38 \text{ h}^{-1}$ at impeller tip speeds between 0.1 and 0.5 m/s and gassing rates between 5 and 25 sL/h. That process operation range covers most mammalian cell culture needs. Higher impeller tip speeds and gassing rates, e.g. 1 m/s and 60 sL/h respectively, led to a greater k_La increase. However, such operation parameters do not represent common mammalian cell cultivation conditions due to greater shear stress for the cells.

The impeller tip speed zone of 0.1 – 0.5 m/s can be used to compare the k_La values of BioBLU Single-Use Bioreactors with different volumes from small to bench scale. For example, the determined k_La values of the BioBLU 1c are comparable and overlap with the k_La values of BioBLU 0.3c (max. working volume 0.25 L), 3c (max. working volume 3.75 L) and 50c (max. working volume: 40 L), which allows the use of constant k_La between different sized vessels as a strategy for cell culture scale-up [4].

Discussion

k_La is an important parameter describing the capacities of a bioreactor to transfer gas into the bioreactor medium and can be used for scale-up strategies. Several methods exist to determine k_La values and different methods may lead to varying k_La values of the same bioreactor [2]. This short protocol introduces a well-accepted k_La determination method, which is accurate, easy, cost-effective, safe, sustainable, and environmentally friendly.

The short protocol presented here is based on DECHEMA recommendations, in which a headspace gas exchange is recommended to reduce the residual nitrogen concentration in the gassing phase and thereby, ensure a more precise

measurement of the oxygen transfer [3]. This short protocol provides an example for users to plot out their own graphs for the calculation of k_La . Alternatively, users can also use a web-based table offered by DECHEMA to automatically calculate the k_La values [3].

In summary, this short protocol describes a reliable and reproducible method for measuring the k_La value of a bioreactor. It can serve as a reference for the bioprocess professionals who are interested in k_La measurements of the large collection of bioreactors within the Eppendorf portfolio including reusable glass and single-use bioreactors of different volumes from small to bench scale.

Literature

- [1] Garcia-Ochoa, F., Gomez, E. (2009). Bioreactor scale-up and oxygen transfer rate in microbial processes: an overview. *Biotechnology advances*, 27(2), 153-176.
- [2] Aroniada, M., Maina, S., Koutinas, A., Kookos, I. K. (2020). Estimation of volumetric mass transfer coefficient ($k_L a$) - Review of classical approaches and contribution of a novel methodology. *Biochemical Engineering Journal*, 155, 107458.
- [3] Bauer, I., Dreher, T., Eibl, D., Glöckler, R., Husemann, et al. (2020). Recommendations for process engineering characterisation of single-use bioreactors and mixing systems by using experimental methods. DECHEMA Gesellschaft für Chemische Technik und Biotechnologie eV.
- [4] Han, X. K., Willard, S., Sha, M. (2016). Cell Culture Scale-Up in BioBLU® c Rigid-Wall, Single-Use Bioreactors. Eppendorf Poster. http://cellculturedish.com/wp-content/uploads/sites/2/2020/05/Poster_BioBLU_Cell-Culture-Scale-U_eng.pdf [17.05.2024]

Ordering information

Description	Order no.
BioBLU® 1c Single-Use Bioreactor, open pipe, 1 pitched-blade impeller, no pH, X-ray, 4 pieces	1386 111 000
DASGIP® Bioblock, 4-position heating/cooling block, max. temp. 99 °C	76DGTBLOCK
DASGIP® TC4SC4 Temperature and Agitation Control Module, for or 4 vessels	76DGTC4SC4B
DASGIP® PH4PO4RD4L Monitoring Module, for 4 vessels, pH, DO and redox with level/anti foam option	76DGPH4PO4RDL
DASGIP® MX4/4 Gas Mixing Module, for 4 vessels, mass flow controller, 0.5 – 250 sL/h, 0.5 – 150 sL/h CO2	76DGMX44H
BioFlo® 320, base control station, with water connection	1379 963 011

Your local distributor: www.eppendorf.com/contact
 Eppendorf SE · Barkhausenweg 1 · 22339 Hamburg · Germany
eppendorf@eppendorf.com · www.eppendorf.com



www.eppendorf.com/bioprocess

Hamilton® is a registered trademark of Hamilton Company, USA. Thermo Fisher Scientific® is a registered trademark of Thermo Fisher Scientific Inc., USA. Eppendorf®, the Eppendorf Brand Design and BioBLU® are registered trademarks of Eppendorf SE, Germany. BioFlo® is a registered trademark of Eppendorf, Inc., USA. DASGIP® is a registered trademarks of DASGIP Information and Process Technology GmbH, Germany. Methods are intended for research applications. They are not intended, verified or validated for use in the diagnosis of disease or other human health conditions. All rights reserved, including graphics and images. Copyright © 2024 by Eppendorf SE, Germany.

Eppendorf SE reserves the right to modify its products and services at any time. This short protocol is subject to change without notice. Although prepared to ensure accuracy, Eppendorf SE assumes no liability for errors, or for any damages resulting from the application or use of this information. Viewing the short protocol alone cannot as such provide for or replace reading and respecting the current version of the operating manual.